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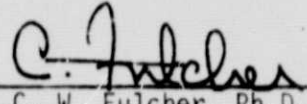

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SUBJECT A Simple Model of Fluid Flow and Electrolyte Balance in the Body			
<p>(NASA-CR-160205) A SIMPLE MODEL OF FLUID FLOW AND ELECTROLYTE BALANCE IN THE BODY (University of Southwestern) 27 p HC A03/MF A01</p> <p style="text-align: right;">N79-25722 CSCL 06P G3/52 Unclas 22194</p> <p>This model is basically a three-compartment model, the three compartments being the plasma, interstitial fluid and cellular fluid. Sodium, potassium, chloride and urea are the only major solutes considered explicitly. The control of body water and electrolyte distribution is affected via drinking and hormone levels. Basically, the model follows the effect of various oral input water loads on solute and water distribution throughout the body.</p> <div style="text-align: right;"> C. W. Fulcher, Ph.D.</div> <div style="text-align: center;"></div> <p>Attachment /db</p>			
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ASD 4028

A SIMPLE MODEL OF FLUID FLOW  
AND  
ELECTROLYTE BALANCE IN THE BODY

BY

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## I. INTRODUCTION

Mathematical modeling of various body functions is a relatively new area of scientific endeavor, dating back only about thirty years. The field of modeling of physiologic processes is interdisciplinary requiring expertise from diverse disciplines for its success. By its very nature, this type of modeling requires considerable pooling of knowledge from applied mathematics, chemistry and physiology. It is all too often true that experts in the area of physical science and experts in the area of life science have little in common that permits them to contribute meaningfully to the same research project. What is superficial or even trivial for one group may be abstruse for the other. It is only through a mutual understanding of the strengths and weaknesses of each group that work in the area of physiological modeling can bear fruit.

This simple model of fluid and electrolyte balance in the human system has been prepared in the hope that it will foster such mutual understanding between those developing models and those ultimately using similar models. The present model, a modification of a basic model<sup>1</sup> of the subsystems regulating fluid and electrolyte balance, allows one to follow the changes in the body accompanying oral ingestion of water. This dynamic model is able to qualitatively predict the changes in twenty-three variables for an average man after varied oral input loads. It is hoped that personnel not familiar with models may learn by actual usage what to expect from simple models and perhaps how to improve them.

## II. THE MODEL

The model for fluid and electrolyte balance is a modification of an earlier developed model<sup>1</sup>. This model is basically a three compartment

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<sup>1</sup>

Superscript refers to Table of References at end of report.

model, the three compartments being the plasma, interstitial fluid and cellular fluid. Sodium, potassium, chloride and urea are the only major solutes considered explicitly. The control of body water and electrolyte distribution is affected via drinking and hormone levels. Basically, the model follows the effect of various oral input water loads on solute and water distribution throughout the body. Figure 1 gives a flow diagram for the model.

#### Solute Distribution and Flow

The processes which govern water and solute flow between various compartments are diffusion, osmosis and ultrafiltration<sup>2,3</sup>. The normal osmolarity of the body fluid,  $O_T^O$ , is taken to be 300 mosmols/l and the normal total body water,  $V_T^O$ , is taken as 40 l. Initial amounts of solutes present are (in mosmols):

$Q_{NA}^O = 5200$ ,  $Q_K^O = 224$ ,  $Q_{CL}^O = 5424$ ,  $Q_U^O = 200$  and  $Q_S^O = 952$  where NA = sodium, K = potassium, CL = chloride, U = urea, and S = other solutes. It is assumed that initially the total solute is evenly distributed throughout the body and that the amount of solute in the cells does not change with time.

The solute loss rate through the feces,  $L_F$ , is assumed constant at 0.03 mosmols/min and similarly the solute loss rate from the lungs and skin,  $L_I$ , is taken as constant at 0.1 mosmols/min. The gain rates of the various solutes (from metabolism) are taken as constant and are (mosmols/min):

$A_{NA} = 0.206$ ,  $A_K = 0.0424$ ,  $A_{CL} = 0.248$ ,  $A_U = 0.376$ , and  $A_S = 0.0403$ . All solutes are assumed to enter the system through the plasma and diffuse into the interstitial space. Losses occur through the urine, feces, lungs and skin.

The material balance equations for the total solute in the plasma and interstitial spaces are (the cells are assumed to have a fixed quantity of solute):

$$\frac{d}{dt} Q_P = A_P^T - L_P^T \quad (1)$$

and

$$\frac{d}{dt} Q_{ISF} = A_{ISF}^T - L_{ISF}^T \quad (2)$$

where  $A_i^T$  and  $L_i^T$  represent total solute gain and loss rates from the relevant compartments. These gain and loss rates are (mosmols/min):

$$A_P^T = A_P^{ISF} + A_{NA} + A_K + A_{CL} + A_U + A_S, \quad (3)$$

$$L_P^T = L_P^{ISF} + L_U + L_F, \quad (4)$$

$$A_{ISF}^T = A_{ISF}^P, \quad (5)$$

and

$$L_{ISF}^T = L_{ISF}^P + L_I. \quad (6)$$

The diffusive gain rate of solute by the plasma from the interstitial space,  $A_P^{ISF}$ , is taken as zero. The diffusive loss of solute from the plasma to the interstitial space,  $L_P^{ISF}$ , is given by the Fick's law result

$$L_P^{ISF} = k_{56} (O_P - O_{ISF}) \quad (7)$$

where  $O_i$  represents the osmolar concentration of solutes in the plasma or interstitial space. The gain rate of solute by the interstitial space is taken to be the same as the loss rate of solute by the plasma to the interstitial space, since the cells do not lose solute in this model. Thus

$$A_{ISF}^T = L_P^{ISF}. \quad (8)$$

Similarly the loss rate  $L_{ISF}^P$  is assumed to be the same as the gain rate  $A_P^{ISF}$  which is zero. Note that  $A_P^T = 0.913$  and  $L_{ISF}^T = 0.1$  mosmols/min.



The total urinary loss rate of solute is given by the sum of the loss rates for the individual species considered. Thus

$$L_U = l_{NA} + l_K + l_{CL} + l_U + l_S \quad (9)$$

where  $l_i$  is the urinary loss rate of species  $i$ . The assumption is made that  $l_S$  is constant

$$l_S = 0.03 \text{ mosmols/l.} \quad (10)$$

Sodium and potassium loss rates are assumed to be controlled by the aldosterone level in the plasma. An additional controlling factor for sodium is the body level of sodium. Note that potassium level does not influence potassium loss directly. It does have an indirect influence by affecting aldosterone production. Hence

$$l_{NA} = M_1 O_{NA}^T - M_2 O_A \quad (11)$$

where  $M_1$  and  $M_2$  are constants and  $O_{NA}^T$  is the osmolarity of sodium in the body,  $O_{NA}^T = \frac{Q_{NA}}{V_T}$ , and  $O_A$  is the aldosterone level (in the plasma). For potassium loss

$$l_K = M_3 O_A \quad (12)$$

where  $M_3$  is constant. Loss of chloride is taken as passive loss caused by charge balance

$$l_{CL} = l_{NA} + l_K \quad (13)$$

Urea loss rate is assumed to depend on the osmolarity of urea in the body and the urinary excretion rate of water. The relationship used is

$$l_U = k_1 \left\{ 1 + k_2 (1 - e^{-k_3 \lambda_P^U}) \right\} O_U \quad (14)$$

where  $O_U$  is the osmolarity of urea in the body,  $O_U = \frac{Q_U}{V_T}$ , and  $\lambda_P^U$  is the urinary excretion rate of water (discussed in Section III).

Material balance is required for the individual solutes just as for the total solute. The relevant equations are

$$\frac{d}{dt} Q_{NA} = A_{NA} - l_{NA} - (L_F + L_I) \frac{Q_{NA}}{Q_T}, \quad (15)$$

$$\frac{d}{dt} Q_K = A_K - l_K - (L_F + L_I) \frac{Q_K}{Q_T}, \quad (16)$$

$$\frac{d}{dt} Q_{CL} = A_{CL} - l_{CL}, \quad (17)$$

$$\frac{d}{dt} Q_U = A_U - l_U - (L_F + L_I) \frac{Q_U}{Q_T}, \quad (18)$$

and

$$\frac{d}{dt} Q_S = A_S - l_S - (L_F + L_I) \frac{Q_S}{Q_T}, \quad (19)$$

where  $Q_T$  is the total amount of solute in the body.

#### Water Distribution and Flow

Oral water ingestion is simulated via a two-compartment system which delays the entrance of water into the plasma. The two compartments, the stomach and intestines, are simply reservoirs from which water flows into the plasma. Thus

$$\frac{dV_S}{dt} = r_I - k_{11} V_S \quad (20)$$

and

$$\frac{dV_G}{dt} = k_{11} V_S - k_{12} V_G \quad (21)$$

where  $V_i$  is the water volume in compartment  $i$  ( $S$  = stomach,  $G$  = gut) and  $r_I$  is the input flow rate of water. This input flow rate is due to salivation and drinking, with drinking occurring only once at time  $T_0$ . Salivation is considered constant at 0.64 ml/min.

From the intestine water flows into the plasma. The assumption is made that the red cell volume is constant. The plasma is in direct contact



with the interstitial space and water flow may also occur because of metabolism, urinary loss and fecal loss. The relevant flow equation is

$$\frac{dV_P}{dt} = a_P^G + a_P^{ISF} + a_P^M - \lambda_P^{ISF} - \lambda_P^U - \lambda_P^F \quad (22)$$

where  $a_P^i$  represents a gain rate of water by the plasma from  $i$  and  $\lambda_P^i$  represents a corresponding loss rate. The superscripts have the meanings: G: gut, ISF: interstitial fluid, M: metabolism, U: urine, F: feces. The metabolic rate of volume gain is considered constant (1.0 ml/min) as is the fecal loss rate (0.1 ml/min). The gain rate from the intestines is

$$a_P^G = k_{12} V_G \quad (23)$$

Water flow between the plasma and interstitial space is assumed to occur by lymph flow and by filtration at the arterial end and reabsorption at the venous end.<sup>3</sup> The lymph flow rate is taken as constant,  $a_P^L = 1.7$  ml/min, and the flow into the plasma from the interstitial space is thus

$$a_P^{ISF} = a_P^L + k_{13} (P_{ISF} - P_V + \pi_P - \pi_{ISF}) \quad (24)$$

where  $k_{13}$  is constant,  $P_{ISF}$  is the hydrostatic pressure of the interstitial space,  $P_V$  is the venous capillary hydrostatic pressure,  $\pi_P$  is the plasma colloid osmotic pressure and  $\pi_{ISF}$  is the interstitial space colloid osmotic pressure. Similarly filtration is given by:

$$\lambda_P^{ISF} = k_{14} (P_A - P_{ISF} + \pi_{ISF} - \pi_P) \quad (25)$$

where  $k_{14}$  is assumed to equal  $k_{13}$  and  $P_A$  is the arterial capillary hydrostatic pressure.  $P_A$  is considered to vary linearly with the total blood volume (red cell volume plus plasma volume)

$$P_A = k_{15} V_B \quad (26)$$

where  $V_B = V_P + V_R$  with  $V_R$ , the volume of the red cells, fixed at 2.0 l.

$$P_V = k_{16} V_B \quad (27)$$

$P_{ISF}$  is taken to be normally negative and is assumed to vary linearly with the volume of the interstitial space

$$P_{ISF} = P_{ISF}^0 + k_{17} (V_{ISF} - V_{ISF}^0) \quad (28)$$

where  $P_{ISF}^0 = -7$  mm Hg and  $V_{ISF}^0 = 12000$  ml. The interstitial oncotic pressure,  $\pi_{ISF}$ , is taken as constant (4.5 mm Hg), but the plasma oncotic pressure,  $\pi_p$ , is assumed to depend linearly on the plasma protein concentration

$$\pi_p = X/V_p \quad (29)$$

where  $X$  is related to the amount of plasma protein.  $X$  is initially taken to be constant but whenever  $\pi_p$  drops below 26 mm Hg (by  $V_p$  increasing) protein is produced at a fixed rate

$$\frac{dX}{dt} = k_{18} \quad (30)$$

until  $\pi_p$  exceeds 26 mm Hg.

The urinary loss rate of water from the plasma,  $\lambda_p^U$ , is assumed to depend on the vasopressin (ADH) level in the plasma,  $C_{ADH}$  ( $= Q_{ADH}/V_p$ ), and on the rate of solute excretion. The kidney is assumed to have different responses to ADH levels depending on past experiences. A sensitivity parameter  $Z$  is created with

$$\frac{dZ}{dt} = Z_1. \quad (31)$$

If  $Z_1 > 0$ , the urine flow rate of water due to ADH effect is

$$\lambda_{p,1}^U = \frac{k_{19}}{k_{20} + C_{ADH}} \quad (32)$$

but if  $Z_1 \leq 0$  this rate increases to

$$\lambda_{p,1}^U = \frac{k_{19}}{k_{20} + C_{ADH}} - Z_1 \left( k_{21} + \frac{k_{22}}{k_{20} + C_{ADH}} \right). \quad (33)$$

The parameter  $Z_1$  has a time-delay mechanism

$$Z_1(t) = Q_{ADH}(t) - k_{23} Z(t-\tau) \quad (34)$$

with  $\tau = 1$  min. The total urinary loss rate of water is, taking solute excretion into account

$$\lambda_P^U = \lambda_{P,1}^U + k_{24} L_U \quad (35)$$

where  $L_U$  is given by Eqn. (9).

For the interstitial space the analogue to Eqn. (22) is

$$\frac{dV_{ISF}}{dt} = a_{ISP}^P - \lambda_{ISF}^P - \lambda_{ISF}^{ICF} - \lambda_{ISF}^I \quad (36)$$

where  $a_{ISP}^P$  is the gain rate in interstitial fluid from the plasma,  $\lambda_{ISF}^P$  is the corresponding loss rate to the plasma,  $\lambda_{ISF}^{ICF}$  is the osmotic flow rate to the cells, and  $\lambda_{ISF}^I$  is the insensible loss rate through the skin and lungs.  $\lambda_{ISF}^I$  is taken as constant (0.5 ml/min),  $a_{ISP}^P = \lambda_P^{ISF}$ , and  $\lambda_{ISF}^P = a_P^{ISF}$ . The rate of volume flow due to osmotic flow to the cells is given by Fick's law

$$\lambda_{ISF}^{ICF} = k_{25} (O_{ICF} - O_{ISF}) \quad (37)$$

where  $O_i$  represents the total osmolarity of  $i$  in mosmols/l.

#### Aldosterone Production

Aldosterone is assumed to be produced via a renin, angiotensin, aldosterone mechanism sensitive to blood volume and potassium level. All three of these substances are considered to be produced by similar means. For aldosterone the relevant expression is

$$\frac{d}{dt} Q_A = k_4 \frac{Q_G}{V_P} + k_5 \frac{Q_K}{V_T} - k_6 Q_A \quad (38)$$

$Q_i$  represents the quantity of  $i$  ( $A$  = aldosterone,  $G$  = angiotensin,  $K$  = potassium,  $R$  = renin). For angiotensin the rate equation is

$$\frac{d}{dt} Q_G = k_7 \frac{Q_R}{V_P} - k_8 Q_G \quad (39)$$

For renin the production rate is taken as zero if the blood volume,  $V_B$ , exceeds 7000 ml. Otherwise

$$\frac{dQ_R}{dt} = k_9 (B_1 - V_B) - k_{10} Q_R \quad (40)$$

where  $B_1 = 7000$  ml.

#### Vasopressin (ADH) Production

The production of ADH is assumed to depend on the blood volume and the plasma osmolarity. The time delay involved in ADH production is simulated by requiring flow through five hypothetical states between initiation of production and flow into the plasma. The rate equations for these five states are

$$\begin{aligned} \frac{dQ_1}{dt} &= K(P_{ADH} - Q_1), \\ \frac{dQ_2}{dt} &= K(Q_1 - Q_2), \\ \frac{dQ_3}{dt} &= K(Q_2 - Q_3), \\ \frac{dQ_4}{dt} &= K(Q_3 - Q_4), \end{aligned} \quad (41)$$

and

$$\frac{dQ_{ADH}}{dt} = Q_4 - k_{26} Q_{ADH}$$

where

$$K = \frac{8}{40 + C_{ADH}}$$

with  $C_{ADH} = Q_{ADH}/V_P$

The initial production rate,  $P_{ADH}$ , has two components

$$P_{ADH} = p_1 + p_2 \quad (42)$$

where  $p_1$  is the production rate due to blood volume and  $p_2$  is the production rate due to plasma osmolarity. In both cases  $p_i$  is taken as non-negative. The form of  $p_1$  is

$$p_1 = k_{27} - k_{28} \Delta_1 - k_{29} \exp(k_{30} \Delta_1) \quad (43)$$

where

$$\Delta_1 = \frac{V_P - V_P^0}{V_B}.$$

The rate  $p_2$  has the form

$$p_2 = k_{31} + k_{32} \Delta_2 - k_{33} \exp(-k_{34} \Delta_2) \quad (44)$$

where

$$\Delta_2 = O_P - O_T^0 \quad (O_T^0 \text{ is the normal total body osmolarity}).$$

### III. NUMERICAL METHODS

Most of the equations of the preceding section are differential and require approximation if a numerical solution is to be obtained. With the exception of Eqns (20) and (21) which are solved exactly, all of the differential equations are solved by using Euler's method. This method has severe limitations as to both accuracy and stability, but it is a very simple method to use and probably does not lead to serious error during the meaningful time durations being examined by the model. The results, however, should be interpreted qualitatively, not quantitatively.

The general form of the differential equations encountered in section II is

$$\frac{d}{dt} y = f(t, y) \quad (45)$$

with some initial condition  $y(t_0)$  specified. Euler's method generates  $y(t_1)$  where  $t_1 = t_0 + h$ , with  $h$  being a fixed parameter called the step size. The function  $y$  is assumed analytic in the vicinity of  $t_0$  ( $y$  has a Maclaurin expansion) so that



$$y(t_0 + h) = y(t_0) + h y'(t_0) + \frac{h^2}{2} y''(t_0) + \dots \quad (46)$$

and  $h$  is assumed small enough so that the terms beyond first order in  $h$  may be neglected. This gives

$$y(t_0 + h) = y(t_0) + h y'(t_0). \quad (47)$$

The Eqn (45) is used to calculate  $y'(t_0)$

$$y'(t_0) = f(t_0, y(t_0)) \quad (48)$$

and this is used in Eqn (47) resulting in

$$y(t_0 + h) = y(t_0) + h f(t_0, y(t_0)). \quad (49)$$

This process is repeated until  $y(t)$  is generated for the  $t$  desired.

In this work  $h = 1$  min. and the reported values of the  $y$  are at 10 minute intervals.

#### IV. THE USE OF THE PROGRAM

A Fortran IV version of this model is listed in Appendix A. This program simulates the changes in levels of the twenty-three quantities listed in Table 1 when a person of average size consumes a quantity of water after having no oral water intake for six hours.

The user of the program may select as many as nine of the twenty-three quantities and have their levels printed out in column form at ten minute increments after consumption of the water (sixty minute increments before consumption).

The program is presently designed to use cards as the input mechanism and printed page (132 columns) as the output mechanism. Each data card should have an integer right justified in card column 5. The integer in the first data card tells the quantity of water consumed (in milliliters). The integer in column 5 of the second data card tells how many (from 1 to 9) columns of information are requested. Then that number of data cards follows, one for each column of information requested, arranged in the order in which

the user wants the columns to be printed. Each of these remaining data cards should have an integer from one to twenty-three right justified to card column 5 together with any appropriate column heading (preferably centered) in columns 10 thru 17 for the quantity which that integer represents, according to the list in Table 1.

The output will consist of a statement of the quantity of water consumed followed by the column headings which the user selected (in the order in which the data cards are arranged) and the levels of these quantities at ten minute increments after the water is consumed. The output may be considered accurate to at most three significant figures in spite of the figures given.

## REFERENCES

1. The basic model was constructed by Thomas G. Cleaver of the University of Louisville.
2. P. H. Abbrecht, Compartments and Body Fluids, Biomed. Engrg. XX:161, 1971.
3. C. A. Widerhielm, Dynamics of Transcapillary Fluid Exchange, Journal Gen. Physiol. 52:29s, 1968.

## APPENDIX A

A Fortran IV Version of a Model which Simulates Fluid  
and Electrolyte Balance in the Body.

C AFTER FASTING FOR 6 HOURS, THE SUBJECT CONSUMES A GIVEN  
 C QUANTITY OF WATER. SPECIFY THIS QUANTITY IN ML AS AN  
 C INTEGER RIGHT JUSTIFIED IN COLUMN 5 OF THE FIRST DATA  
 C CARD.  
 C  
 C FROM THE FOLLOWING LIST YOU MAY SELECT AS MANY AS NINE OF  
 C THE TWENTY-THREE QUANTITIES THAT YOU ARE INTERESTED IN.  
 C THE PRINT OUT WILL CONSIST OF A COLUMN OF THE INDEPENDENT  
 C TIME VARIABLE IN TEN MINUTE INCREMENTS AFTER CONSUMPTION  
 C (60 MIN INCREMENTS BEFORE CONSUMPTION) FOLLOWED BY  
 C COLUMNS OF THE INFORMATION THAT YOU REQUEST, IN THE ORDER  
 C IN WHICH THEY ARE REQUESTED, AT EACH TEN MINUTE  
 C INCREMENT. THE INPUT SHOULD CONSIST OF A SECOND DATA  
 C CARD HAVING AN INTEGER FROM 1 TO 9 IN COLUMN 5 TELLING  
 C HOW MANY QUANTITIES YOU SELECT, FOLLOWED BY THAT  
 C NUMBER OF DATA CARDS, EACH HAVING AN INTEGER FROM 1  
 C TO 23 RIGHT JUSTIFIED IN COLUMN 5 TOGETHER WITH ANY  
 C APPROPRIATE COLUMN HEADING (PREFERABLY CENTERED) IN  
 C COLUMNS 10 THRU 17 FOR THE QUANTITY WHICH THAT INTEGER  
 C REPRESENTS, ACCORDING TO THE FOLLOWING LIST:  
 C 1 - VOL OF WATER IN STOMACH  
 C 2 - VOL OF WATER IN INTESTINES  
 C 3 - VOL OF WATER IN PLASMA  
 C 4 - VOL OF WATER IN INTERSTITIAL FLUID  
 C 5 - VOL OF WATER IN CELL FLUID  
 C 6 - TOTAL WATER VOLUME IN PLASMA, INTERSTITIAL SPACE,  
 C AND CELLS  
 C 7 - RATE OF PRODUCTION OF URINE  
 C 8 - TOTAL SOLUTE IN PLASMA  
 C 9 - TOTAL SOLUTE IN INTERSTITIAL FLUID  
 C 10 - TOTAL SOLUTES IN PLASMA, INTERSTITIAL SPACE,  
 C AND CELLS  
 C 11 - RATE OF PRODUCTION OF SOLUTES IN URINE  
 C 12 - ADH  
 C 13 - RENIN  
 C 14 - ANGIOTENSIN  
 C 15 - ALDOSTERONE  
 C 16 - SODIUM LOSS  
 C 17 - POTASSIUM LOSS  
 C 18 - CHLORIDE LOSS  
 C 19 - UREA LOSS  
 C 20 - PLASMA OSMOLARITY  
 C 21 - INTERSTITIAL FLUID OSMOLARITY  
 C 22 - CELL FLUID OSMOLARITY  
 C 23 - URINE OSMOLARITY  
 C  
 C VOLUME IS GIVEN IN ML, TIME IN MINUTES, AMOUNTS OF SOLUTE  
 C IN MILLIOSMOLS, AND OSMOLARITY IN MILLIOSMOLS/LITER  
 C  
 C\*\*\*\* THIS IS THE PROGRAM FOR BODY WATER AND ELECTROLYTE  
 C\*\*\*\* BALANCE. VARIABLES AND CONSTANTS USED IN THIS PROGRAM  
 C\*\*\*\* WILL BE USED ACCORDING TO THE FOLLOWING FORMAT.



```

C**** ALPHABETIC VARIABLES AND CONSTANTS
C**** A - ALDOSTERONE
C**** B - BLOOD VOLUME
C**** C - CHLORIDE
C**** D - DELTA T (THE INTEGRATING TIME INTERVAL)
C**** E - ERYTHROCYTE VOLUME
C**** F
C**** G - ANGIOTENSIN
C**** H - ADH
C**** I - CONSTANTS RELATED TO CAPILLARIES
C**** J - CONSTANTS RELATED TO CELL-INTERSTITIAL INTERFACE
C**** K - POTASSIUM (MILLIOSMOLS)
C**** L - CONSTANTS RELATED TO ADH PRODUCTION
C**** M - CONSTANTS RELATED TO ALDOSTERONE PRODUCTION
C**** N - SODIUM (MILLIOSMOLS)
C**** O - OSMOLARITY (MILLIOSMOLS/LITER)
C**** P - PRESSURE (MILLIMETERS OF MERCURY)
C**** Q - TOTAL SOLUTE (MILLIOSMOLS)
C**** R - RENIN
C**** S - SOLUTE OTHER THAN NA, K, CL, U (MILLIOSMOLS)
C**** T - TIME CONSTANT OR TIME (MINS)
C**** U - UREA (MILLIOSMOLS)
C**** V - VOLUME (MILLILITERS)
C**** W - CONSTANTS RELATED TO THE KIDNEY
C**** X - PLASMA PROTEIN
C**** Y - CONSTANTS RELATING URINE OUTPUT TO UREA OUTPUT
C**** Z - A MEASURE OF KIDNEY SENSITIVITY TO ADH
C**** SUBSCRIPTS
C**** 0 - AVERAGE, DESIRED OR REFERENCE VALUE
C**** 1 - D/DT (TIME DERIVATIVE)
C**** 2 - EXTERNAL INPUT OR OUTPUT
C**** 3 - STOMACH
C**** 4 - INTESTINE
C**** 5 - PLASMA
C**** 6 - INTERSTITIAL FLUID
C**** 7 - CELL FLUID
C**** 8 - URINE
C**** 9 - OTHER
C
C      NOMLWC IS THE NUMBER OF ML. OF WATER CONSUMED.
      READ (5,2000) NOMLWC
2000  FORMAT(15)
      WRITE (6,2010) NOMLWC
2010  FORMAT(34X,'AFTER FASTING FOR 6 HOURS, THE SUBJECT'
      *' CONSUMES',15,1X,'ML OF WATER.'/)
C      VWC = VOLUME OF WATER CONSUMED = NOMLWC
      VWC=NOMLWC
      REAL  L0,L1,L2,L3,L4,L5,M1,M2,M3,M4,M5,M6,M7,M8,N3,K3,N2
      REAL  V(167),Q(167),O(9),N,K,I1,I2,I3,I4,I5,I6,J,K2,N1
      REAL  K34,K45
C
      DIMENSION COL(23), ALPHA(9), BETA(9)

```

```

C      NREQ = NUMBER OF COLUMNS OF INFORMATION REQUESTED
      READ (5,2200) NREQ
      2200 FORMAT(I5)
C***** INITIALIZE VARIABLES AND DEFINE CONSTANTS **
C****
C**** THE SUBJECT TAKES A DRINK OF WATER AT TIME T5
      T5 = 361.
C**** V(50), V(60) AND V(70) ARE THE NORMAL VALUES OF THE
C**** PLASMA, INTERSTITIAL FLUID AND CELLS, RESPECTIVELY IN ML
C      ACCORDING TO GUYTON'S TEXTBOOK OF MEDICAL PHYSIOLOGY,
C      V(50)=3000, V(60)=12000, V(70)=25000, AND E=2000 ML.
C      V(50) = 3200.
C      V(50) = 3000.
C      V(60) = 13800.
C      V(60) = 12000.
C      V(70) = 28000.
C      V(70) = 25000.
C**** Q0 IS THE NORMAL OSMOLARITY OF BODY FLUID IN MOSMOL/LITER
      Q0 = 300.
C**** V(90) IS NORMAL TOTAL BODY WATER
      V(90)=V(50)+V(60)+V(70)
C**** Q IS THE INTEGRATING INTERVAL IN MINUTES
      Q=1.
C**** V(23) IS THE INPUT WATER LOAD
C      V(23)=.64
C      .64 ML/MIN OF WATER ARE SWALLOWED IN SALIVA.
      RATE=.64
C**** N, K, C, AND U ARE THE TOTAL AMOUNTS OF THE SOLUTES NA,
C**** K, CL AND UREA DISSOLVED IN THE BODY FLUIDS, RESPECTIVELY
C***** GENERAL *****
      N=V(90)*130./1000.
      K=V(90)*5.1/1000.
      C=N+K
      U=V(90)*5.0/1000.
C**** S IS ALL OTHER SOLUTES IN THE BODY FLUID
      S=(Q0/1000.)*V(90)-N-K-C-U
C**** Q(9) IS THE TOTAL INITIAL SOLUTE IN THE BODY
      Q(9)=N+K+C+U+S
C**** V(34) IS THE VOLUME THAT HAS FLOWED FROM STOMACH TO
C**** INTESTINE IN ML
C***** STOMACH *****
C      V(34)=0.
      T3=20.
      K34=1./T3
C***** GUT *****
C      V(45)=0.
      T4=18.
      K45=1./T4
C***** BLOOD *****
      V(156)=0.
      V(165)=0.
      V(18)=0.

```

```

V(159)=.1
V(125)=1.
V(5)=V(50)
Q(156)=0.
Q(165)=0.
V(18)=0.
Q(159)=Q0*V(159)/1000.
Q(5)=Q(9)*V(50)/V(90)
C***** INTERSTITIAL FLUID *****
V(167)=0.
V(162)=.5
Q(162)=.2*V(162)
V(6)=V(60)
Q(6)=Q(9)*V(60)/V(90)
C***** CELLS *****
V(7)=V(70)
Q(7)=Q(9)*V(70)/V(90)
C***** CAPILLARIES *****
C
E=3000.
E=2000.
P0=E+V(50)
I1=25.3/P0
I2=9.0/P0
P6=-7.
I3=1./280.
X2=67.
P7=26.
X=28.0*V(50)
I4=1.7
P5=4.5
I5=1.7
I6=1400.
C***** ADH *****
J=300.
L0=.7
L1=20.
L2=90./L0
L3=00
L4=.2
L5=1440./L0
I6=600.
I7=46
I8=H6
I9=H6
I5=5.0*V(50)
I9=24.4
C***** ALDOSTERONE *****
I1=7000.
I0=100.
I1=I0
I2=I0
I1=V(50)

```

```

M2=V(50)
M3=V(50)
M4=(.755-.148)/(T0*T1*T2*(R1-B0))
R2=M1*(R1-B0)*T0
G2=R2*M2*T1/V(50)
A2=G2*M3*T2/V(50)
M6=.04/((R1-B0)*T0*T1*T2)
M7=(1.0/.0051)*A2/T2
M8=.5
M5=.755*V(20)/N
(***** KIDNEY *****)
H=5.
T8=180.
Z=H*T8
M1=3.
M2=.4
M3=.8
Y1=50.
Y2=1.5
Y3=.3
M3=.15+.13*N/Q(9)
K3=.04+.13*K/Q(9)
C3=N3+K3
M3=.32+.13*N/Q(9)
S3=.03+.13*S/Q(9)
U(125)=N3+K3+C3+U3+S3
M2=0.
K2=N2
U2=N2
C2=N2
S2=.03
(***** STOMACH *****)
C    DO 3900 NT=1,1701
C    DO 3900 NT=1,1061
C    T=NT
C    IF (T-T5) 2230,2220,2220
C2220 V(23)=1500
C2230 V(3)=V(23)-V(34)
C    V(3)=(RATE/K34)*(1.-EXP(-K34*T))
C    IF (T-T5) 2230,2220,2220
C2220 V(3)=V(3)+VWC*EXP(-K34*(T-T5))
C    V(134)=V(3)/T3
C    V(34)=V(34)+V(134)*D
(***** GUT *****)
C    V(4)=V(34)-V(45)
C2230 V(4)=(K34*RATE/(K45-K34))*((1./K34)*(1.-EXP(-K34*T))-
C    * (1./K45)*(1.-EXP(-K45*T)))
C    IF (T-T5) 2250,2240,2240
C2240 V(4)=V(4)+(K34*VWC/(K45-K34))*(EXP(-K34*(T-T5))-
C    * EXP(-K45*(T-T5)))
C    V(145)=V(4)/T4
C2250 V(145)=V(4)/T4

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C      V(45)=V(45)+V(145)*D
C***** BLOOD *****
V(15)=V(145)+V(165)-V(156)-V(18)+V(125)-V(159)
V(5)=V(5)+V(15)*D
Q(15)=Q(165)-Q(156)-Q(18)+Q(125)-Q(159)
Q(5)=Q(5)+Q(15)*D
I(5)=Q(5)*1000./V(5)
C***** INTERSTITIAL SPACE *****
V(16)=V(156)-V(165)-V(167)-V(162)
V(6)=V(6)+V(16)*D
Q(16)=Q(156)-Q(165)-Q(162)
Q(6)=Q(6)+Q(16)*D
I(6)=Q(6)*1000./V(6)
C***** CELLS *****
V(17)=V(167)
V(7)=V(7)+V(17)*D
Q(7)=Q(7)*1000./V(7)
C***** CAPILLARIES *****
V(7)=V(5)+V(6)+V(7)
B=E+V(5)
P1=I1*R
P2=I2*R
P3=P6+I3*(V(6)-V(60))
P4=X/V(5)
IF (P4-P7) 2790,2800,2800
2790 X=X+X2*D
2800 V(156)=I4*(P1-P3-P4+P5)**2/(P1-P2)
V(165)=I4*(P2-P3-P4+P5)**2/(P1-P2)+I5
Q(156)=I6*(U(5)-U(6))/1000.
C***** CELL-INTERSTITIAL INTERFACE *****
V(167)=J*(I(7)-Q(6))/1000.
C***** ADH *****
H1=(1.-L0)*(L2*(B0*B0/B+L1-U0)-L5*EXP(L4*(L3-B0*B0/B)))
H2=L0*(L2*(U(5)+L1-U0)-L5*EXP(L4*(L3-U(5))))
IF (H2) 3040,3050,3050
3040 H2=0.
3050 IF (H1) 3060,3070,3070
3060 H1=0.
3070 H3=H1+H2
T6=20.0+H/2.
H6=H6+(H3-H6)*D*4.0/T6
H7=H7+(H6-H7)*D*4.0/T6
H8=H8+(H7-H8)*D*4.0/T6
H9=H8+(H8-H9)*D*4.0/T6
H5=H5+(H9-H5/T9)*D
U=I5/V(5)
C***** ANGIOTENSIN *****
P1=M1*(B1-B)
IF (R1) 3310,3320,3320
3310 R1=0.
3320 P2=R2+(R1-P2/T0)*D
Q=R2/V(5)

```



```

G1=M2*F
G2=G2+(G1-G2/T1)*D
G=G2/V(5)
A1=H8*-3*G+(1.0-H8)*M7*K/V(9)
A2=A2+(A1-A2/T2)*G
A=A2/V(5)
H1=M4*A
H2=M5*N/V(9)-H1
IF (N2) 3430,3440,3440
3430 H2=0.
3440 K2=M6*A
C***** KIDNEY *****
Z1=H-Z/T8
Z=7+Z1*D
IF (Z1) 3530,3530,3527
3527 Z1=0.
3530 V(18)=W1/(W2+H)+(1.05+1.0/(W2+H))*(-Z1)*W3
IF (V(18)) 3550,3560,3560
3550 V(18)=0.
3560 H2=Y1*(1.0+Y2*(1.0-EXP(-Y3*V(18))))*U/V(9)
C2=H2+K2
Q(18)=H2+K2+C2+U2+S2
V(18)=V(18)+Q(18)*1000./1600.
H2=Y1*(1.0+Y2*(1.0-EXP(-Y3*V(18))))*U/V(9)
Q(18)=H2+K2+S2+U2+C2
Q(18)=Q(18)*1000./V(18)
H=(Q(159)+Q(162))/Q(9)
I=I+(N3-N2-H*Q8)*D
K=K+(K3-K2-K*Q8)*D
C=C+(C3-C2)*D
U=U+(U3-U2-U*Q8)*D
S=S+(S3-S2-S*Q8)*D
Q(9)=N+K+C+U+S
C***** PRINT OUT *****
COL(1)=V(3)
COL(2)=V(4)
COL(3)=V(5)
COL(4)=V(6)
COL(5)=V(7)
COL(6)=V(9)
COL(7)=V(18)
COL(8)=Q(5)
COL(9)=Q(6)
COL(10)=Q(9)
COL(11)=Q(18)
COL(12)=H
COL(13)=R
COL(14)=G
COL(15)=A
COL(16)=N2
COL(17)=K2
COL(18)=C2

```

```

      COL(19)=02
      COL(20)=0(5)
      COL(21)=0(6)
      COL(22)=0(7)
      COL(23)=0(8)
      IF(T-1.) 3700,3605,3700
3605 GO 3619 IT=1,NOREQ
      READ (5,3610) NUMBER, ALPHA(IT),BETA(IT)
3610 FORMAT(15,4X,2A4)
      GO TO (3611,3612,3613,3614,3615,3616,3617,3618,3619),IT
3611 NC1=NUMBER
3612 NC2=NUMBER
3613 NC3=NUMBER
3614 NC4=NUMBER
3615 NC5=NUMBER
3616 NC6=NUMBER
3617 NC7=NUMBER
3618 NC8=NUMBER
3619 NC9=NUMBER
      GO TO(3621,3622,3623,3624,3625,3626,3627,3628,3629),NOREQ
3621 WRITE (6,3631) ALPHA(1),BETA(1)
      GO TO 3700
3622 WRITE(6,3632) (ALPHA(IS),BETA(IS), IS=1,2)
      GO TO 3700
3623 WRITE(6,3633) (ALPHA(IS),BETA(IS), IS=1,3)
      GO TO 3700
3624 WRITE(6,3634) (ALPHA(IS),BETA(IS), IS=1,4)
      GO TO 3700
3625 WRITE(6,3635) (ALPHA(IS),BETA(IS), IS=1,5)
      GO TO 3700
3626 WRITE(6,3636) (ALPHA(IS),BETA(IS), IS=1,6)
      GO TO 3700
3627 WRITE(6,3637) (ALPHA(IS),BETA(IS), IS=1,7)
      GO TO 3700
3628 WRITE(6,3638) (ALPHA(IS),BETA(IS), IS=1,8)
      GO TO 3700
3629 WRITE(6,3639) (ALPHA(IS),BETA(IS), IS=1,9)
3631 FORMAT(57X,'TIME'7X,2A4/)
3632 FORMAT(50X,'TIME'7X,2A4,6X,2A4/)
3633 FORMAT(43X,'TIME'7X,2A4,2(6X,2A4)/)
3634 FORMAT(36X,'TIME'7X,2A4,3(6X,2A4)/)
3635 FORMAT(29X,'TIME'7X,2A4,4(6X,2A4)/)
3636 FORMAT(22X,'TIME'7X,2A4,5(6X,2A4)/)
3637 FORMAT(15X,'TIME'7X,2A4,6(6X,2A4)/)
3638 FORMAT( 8X,'TIME'7X,2A4,7(6X,2A4)/)
3639 FORMAT( 1X,'TIME'7X,2A4,8(6X,2A4)/)
C      F1=T-1.
3700 F1=T-1.
      IF (T-(T5-10.)) 3720,3740,3740
3720 F2=F1/60.
C      F6=F1
      GO TO 3750

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```

3740 F2=F1/10.
C F6=T-T5
3750 IF3=F2
3750 IF6=T-T5
      IF3=F2
      F3=IF3
      F4=F3-F2
      IF (F4) 3900,3800,3900
3800 GO TO(3801,3802,3803,3804,3805,3806,3807,3808,3809),NDREQ
3800 WRITE (6,3810) F6,V(5),D(5),V(18),D(8),H
3800 WRITE (108,3810) F6,V(5),D(5),V(18),D(8),H
3810 FORMAT (6F15.5)
3901 WRITE (6,3811) IF6,COL(NC1)
      GO TO 3900
3802 WRITE (6,3812) IF6,COL(NC1),COL(NC2)
      GO TO 3900
3803 WRITE (6,3813) IF6,COL(NC1),COL(NC2),COL(NC3)
      GO TO 3900
3804 WRITE (6,3814) IF6,COL(NC1),COL(NC2),COL(NC3),COL(NC4)
      GO TO 3900
3805 WRITE (6,3815) IF6,COL(NC1),COL(NC2),COL(NC3),COL(NC4),
      *COL(NC5)
      GO TO 3900
3806 WRITE (6,3816) IF6,COL(NC1),COL(NC2),COL(NC3),COL(NC4),
      *COL(NC5),COL(NC6)
      GO TO 3900
3807 WRITE (6,3817) IF6,COL(NC1),COL(NC2),COL(NC3),COL(NC4),
      *COL(NC5),COL(NC6),COL(NC7)
      GO TO 3900
3808 WRITE (6,3818) IF6,COL(NC1),COL(NC2),COL(NC3),COL(NC4),
      *COL(NC5),COL(NC6),COL(NC7),COL(NC8)
      GO TO 3900
3809 WRITE (6,3819) IF6,COL(NC1),COL(NC2),COL(NC3),COL(NC4),
      *COL(NC5),COL(NC6),COL(NC7),COL(NC8),COL(NC9)
3811 FORMAT(57X,14, F14.2)
3812 FORMAT(50X,14,2F14.2)
3813 FORMAT(43X,14,3F14.2)
3814 FORMAT(36X,14,4F14.2)
3815 FORMAT(29X,14,5F14.2)
3816 FORMAT(22X,14,6F14.2)
3817 FORMAT(15X,14,7F14.2)
3818 FORMAT( 8X,14,8F14.2)
3819 FORMAT( 1X,14,9F14.2)
3900 CONTINUE
      STOP
      END

```

TABLE 1. POSSIBLE OUTPUTS OBTAINABLE WITH THIS MODEL

( $\emptyset$  means blank space.)

Number (Columns 4 & 5)	Suggested Headings (Columns 10 thru 17)	Quantity (Units)
1	BELLY $\emptyset$ V $\emptyset$	Vol. of water in stomach (ML)
2	$\emptyset$ GUT $\emptyset$ V $\emptyset$ $\emptyset$	Vol. of water in intestines (ML)
3	PLASMA $\emptyset$ V	Vol. of water in plasma (ML)
4	INTER $\emptyset$ V	Vol. of water in interstitial space (ML)
5	CELL $\emptyset$ F $\emptyset$ V	Vol. of water in cell fluid (ML)
6	TOTAL $\emptyset$ V $\emptyset$	Total water vol. in above 3 (ML)
7	U $\emptyset$ ML/MIN	Rate or production of urine (ML/MIN)
8	PLASMA $\emptyset$ S	Total solute in plasma (m Osmols)
9	INTER $\emptyset$ S	Total solute in interstitial space (m Osmols)
10	ALL $\emptyset$ SOL $\emptyset$	Total solute in plasma, interstitial space and cells (m Osmols)
11	U $\emptyset$ S $\emptyset$ RATE	Rate of production of solutes in urine (m Osmols/Min)
12	$\emptyset$ $\emptyset$ $\emptyset$ ADH $\emptyset$ $\emptyset$	ADH
13	$\emptyset$ RENIN $\emptyset$ $\emptyset$	Renin
14	ANGIOTEN	Angiotensin
15	ALDOSTER	Aldosterone
16	$\emptyset$ NA $\emptyset$ LOSS	Sodium Loss Rate (m Osmols/Min)
17	$\emptyset$ $\emptyset$ K $\emptyset$ LOSS	Potassium Loss Rate (m Osmols/Min)
18	$\emptyset$ $\emptyset$ CL $\emptyset$ LOSS	Chloride Loss Rate (m Osmols/Min)
19	UREA $\emptyset$ LOSS	Urea Loss Rate (m Osmols/Min)
20	PLASMA $\emptyset$ O	Plasma Osmolarity (m Osmols/Liter)
21	INTER $\emptyset$ O	Interstitial Osmolarity (m Osmols/Liter)
22	CELL $\emptyset$ F $\emptyset$ O	Cell Fluid Osmolarity (m Osmols/Liter)
23	URINE $\emptyset$ O $\emptyset$	Urine Osmolarity (m Osmols/Liter)



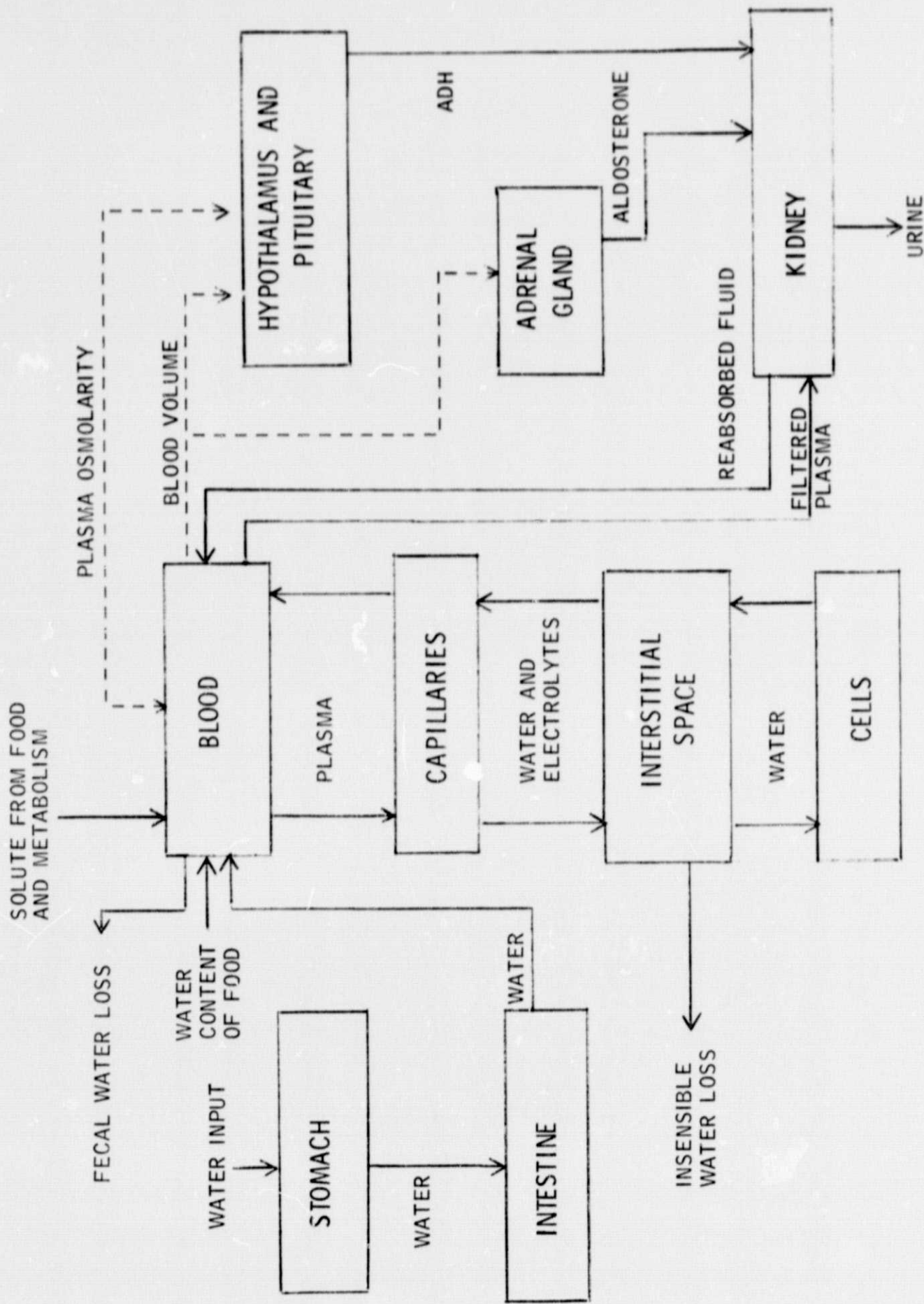


FIGURE 1. GENERAL FLOW CHART OF WATER AND ELECTROLYTE BALANCE.